

A COMPARITIVE STUDY OF MACHINE LEARNING ALGORITHMS FOR DETECTION OF PARKINSON'S DIEAESE AT AN EARLY STAGE

Abstract

Parkinson's disease (PD) is one among many leading public health diseases in the world. This disease has impacted many people and is alarmingly increasing. Thus, it is very important to predict it at an early stage and has been a difficult task among researchers as the symptoms of the disease are evident in either mid or late stages. Thus, this chapter concentrates on the symptoms of speech articulation difficulty of persons with PD and formulates the model using various machine learning like support vector machine, decision tree, random decision forest, and linear regression, adaptive boosting, bagging, neural networks. The performance of these graders is assessed through various measurements, e.g. Accuracy, receptor operating characteristics (ROC) curve, sensitivity, Precision, as well as specificity. Finally, xgboost is used to find the most important features of any feature to predict Parkinson's disease.

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I. INTRODUCTION

Parkinson's disease (PD) is a long-term degenerative disorder of the central nervous system that causes a variety of symptoms to tremors to cognitive disability, hallucination, sleep disorders, etc. Over 10 million people worldwide are affected by Parkinson's disease. In the world every year, approximately 100 thousand people die from Parkinson's disease.

Until now, there has been no cure for PD. However, approximately 10 years before the onset of tremors or motor symptoms, The human brain has Dopaminergic neurons which are the main source of dopamine (DA) in the central nervous system. The change or loss of these neurons is associated with the neurological disorders. Certain premotor symptoms of PD (at an early stage) include a reduction in sense of smell, the disruption in Rapid Eye Movement (REM) sleep, handwriting, difficulty in moving etc.

Early PD diagnosis makes it possible to effectively manage and avoid unnecessary medical tests, therapies, costs, safety risks, etc.. Early stage Parkinson's disease is most often detected using brain studies such as MRI, fMRI, SPECT, PET, etc. So far, in most centers, clinicians are interpreting these images which is prone to human error. It was reported that the pooled accuracy of clinical diagnosis of Parkinson's disease is only 80.6%.

II. LITRATURE SURVEY

We collected handwritten samples and used each sample to extract a handwritten scale [9]. New entropy based handwriting measures, signal energy, and empirical mode decomposition of handwriting signals were computed in addition to conventional kinematic and spatiotemporal handwriting measurements. The maximal sensitivity and specificity for PD categorization were 89.47% and 91.89%, respectively, with an accuracy of up to 88.13% [9]. A useful marker for diagnostic and screening purposes is handwriting. Evaluation of speech captured by cellphones in Parkinson's disease using freely accessible pitch detection algorithms at various noise levels. measurement of the vocal fold's fundamental frequency The assessment of language impairment in Parkinson's disease has identified F0 as a crucial criterion (PD). Pitch Determination Algorithms (PDA) are a broad category of techniques for F0 estimate. The purpose of the study was to examine and compare the performance of several PDAs [1]. Different PDAs which they have examined were:

- Harvest
- RAPT
- PRAAT
- Swipe
- SHRP

To evaluate the PDA's tolerance to additional background noise, they added five distinct types of nonstationary noise to each recording at SNR levels of 20, 10, and 6 dB, respectively. The 6 dB restriction was chosen because it represents the worst-case scenario that is most likely to occur in a typical circumstance [1]. When employing a smartphone device for recording, the SWIPE algorithm can measure mono pitch accurately even in non-stationary urban noise with an SNR of up to 10 dB. To obtain sufficient robustness at lower

SNR levels, a variety of techniques may need to be combined. SWIPE mono pitches have a significant ability to detect PDs.

SNR 6 dB		HARVEST	RAFT	PRAAT AC	PRAAT SHS	REAPER	YANGaf	SHRP	SWIPE	BANA	YAAPT
Noise condition 1											
Mean	MAE	0.75	1.32	0.88	1.87	3.21	0.76	2.38	0.64	0.80	1.82
	NRMSE	0.09	0.17	0.10	0.27	0.37	0.07	0.43	0.05	0.07	0.22
	Spearman r	0.98	0.90	0.93	0.93	0.85	0.97	0.90	0.98	0.97	0.82
SD	MAE	1.87	1.72	0.69	1.96	2.47	1.75	3.02	0.29	0.98	1.51
	NRMSE	0.58	0.34	0.21	0.43	0.55	1.08	0.77	0.10	0.31	0.33
	Spearman r	0.72	0.52	0.64	0.59	0.42	0.65	0.55	0.92	0.58	0.59
Noise condition 2											
Mean	MAE	0.60	0.72	1.79	0.97	2.98	0.94	1.81	0.75	2.54	0.89
	NRMSE	0.07	0.11	0.21	0.15	0.36	0.07	0.39	0.06	0.20	0.12
	Spearman r	0.99	0.92	0.88	0.95	0.82	0.98	0.86	0.98	0.86	0.88
SD	MAE	1.92	1.82	1.70	2.01	2.41	1.50	3.25	0.50	2.98	0.46
	NRMSE	0.58	0.42	0.35	0.57	0.52	0.60	1.04	0.19	0.65	0.12
	Spearman r	0.66	0.55	0.33*	0.74	0.43	0.55	0.57	0.68	0.02*	0.83
Noise condition 3											
Mean	MAE	0.48	0.56	0.66	0.91	1.17	0.14	1.01	0.25	0.40	0.42
	NRMSE	0.05	0.08	0.08	0.11	0.14	0.01	0.14	0.02	0.04	0.08
	Spearman r	0.99	0.92	0.95	0.95	0.92	0.99	0.95	0.99	0.98	0.92
SD	MAE	1.11	0.76	0.93	1.13	1.10	0.25	2.27	0.19	0.53	0.28
	NRMSE	0.36	0.21	0.24	0.34	0.31	0.12	0.74	0.07	0.20	0.12
	Spearman r	0.87	0.76	0.48	0.78	0.77	0.90	0.65	0.95	0.78	0.87
Noise condition 4											
Mean	MAE	0.26	0.49	0.66	0.39	0.65	0.12	0.87	0.32	0.74	0.38
	NRMSE	0.02	0.08	0.06	0.05	0.09	0.01	0.11	0.03	0.06	0.07
	Spearman r	0.99	0.92	0.96	0.97	0.93	0.99	0.95	0.99	0.97	0.93
SD	MAE	0.89	0.54	0.56	0.85	0.74	0.21	2.29	0.23	0.55	0.31
	NRMSE	0.24	0.20	0.20	0.23	0.24	0.09	0.68	0.08	0.23	0.11
	Spearman r	0.87	0.76	0.60	0.81	0.85	0.93	0.61	0.96	0.55	0.88
Noise condition 5											
Mean	MAE	0.37	2.25	2.01	0.40	1.25	0.13	1.90	0.25	1.09	0.43
	NRMSE	0.04	0.21	0.17	0.07	0.14	0.01	0.24	0.02	0.09	0.07
	Spearman r	0.99	0.85	0.85	0.95	0.91	0.99	0.90	0.99	0.93	0.92
SD	MAE	1.26	4.70	2.79	1.48	1.49	0.24	3.39	0.15	1.58	0.29
	NRMSE	0.38	0.56	0.49	0.39	0.39	0.11	0.86	0.06	0.33	0.12
	Spearman r	0.82	0.16*	0.10**	0.75	0.69	0.92	0.31*	0.95	0.35	0.87

MAE = mean absolute error, NRMSE = normalized root mean square error, SD = standard deviation. All correlations reached significance $p < 0.001$ except for * and ** which

Figure 1: Factors Affecting Voice of the Normal Person

A more accurate Parkinson's diagnosis is always preferred to ensure that the right steps are taken to decrease the disease's progression and enhance quality of life. There is evidence that older people and adults have different neural characteristics from men and women. In this paper [5], they developed a sex-specific and age-dependent classification method to diagnose Parkinson's disease using the online handwriting recorded from individuals with Parkinson's ($n = 37$; m/f-19/18; age-69.310.9yrs) and healthy controls ($n = 38$; m/f-20/18; age- 62.411.3yrs). However, the potential of such gender and age information have not yet been exploited for Parkinson's identification.

An SVM ranking algorithm is used to show the characteristics specific to their dominance in sex and age group for Parkinson's diagnosis. It was discovered that the generalised classifier performed significantly worse than the sex- and age-specific classifiers [5]. The female-specific classifier's accuracy was observed to be 83.75% (SD = 1.63) and 79.55% (SD = 1.58), respectively, in compared to the general classifier's accuracy of 75.76% (SD = 1.17) and 79.55% (SD = 1.58). Combining the sex and age information was found to improve categorisation [5]. A specific set of traits was demonstrated to be predominating in a different classification category for increased classification accuracy.

Parkinson's disease (PD) is a progressive neurological disorder that causes both motor and non-motor symptoms. PD patients frequently experience vocal problems early on in the course of the disease. Therefore, diagnostic techniques based on voice issues have received a lot of attention in new PD detection investigations. This paper proposes two convolutional neural network-based frameworks for categorising Parkinson's disease (PD) using sets of vocal (voice) features. Both frameworks are used to merge several feature sets, although they go about it in different ways [7]. While the second architecture passes feature sets to parallel

input layers that are directly connected to convolution layers [7], the first framework integrates different feature sets before transferring them as inputs to a 9-layered CNN. As a consequence, deep features are simultaneously extracted from each parallel combination before being pooled in the merge layer. The proposed models are evaluated using Leave-One-Person-Out Cross Validation after being trained on data from the UCI Machine Learning Repository. (LOPO CV). F-Measure and Matthews Correlation Coefficient metrics are employed for the assessment along with accuracy due to the unbalanced class distribution in our data.

Voice fundamental frequency, measurements of fundamental frequency variation, amplitude variation measurements, etc. are commonly extracted features. Since most PD detection research conducts experiments using both datasets, the features derived from both datasets are commonly referred to as baseline features. In addition to the baseline features, other features based on signal processing techniques were applied in PD identification. Using techniques like the signal-to-noise ratio (SNR), Mel-frequency cepstral coefficients (MFCC), and tunable Q-factor Wavelet Transform (TQWT), it is crucial to be able to extract relevant features for PD classification. Rather than using different feature types for model training, the majority of research incorporates individual feature types to perform classification tasks [7].

The DNN model's accuracy rate of 85% exceeded the typical clinical diagnosis accuracy of non-experts, which was roughly 73.8%. The CNN model worked well, with rates of accuracy, sensitivity, and specificity of 88.25%, 84.71%, and 91.77%, respectively [7]. By merging feature subsets and then utilising mRMR feature selection to choose the informative features, the model produced an accuracy rate of 0.869, an F-Measure of 0.917, and an MCC of 0.632.

Feature Description	Abbreviations
Average vocal fundamental frequency	MDVP:F0 (Hz)
Maximum vocal fundamental frequency	MDVP:PHI (Hz)
Minimum vocal fundamental frequency	MDVP:FLO (Hz)
MDVP jitter in percentage	MDVP:ITTER(%)
MDVP absolute jitter in ms	MDVP:JITTER(ABS)
MDVP relative amplitude perturbation	MDVP:RAP
MDVP five-point period perturbation quotient	MDVP:PPQ
Average absolute difference of differences between jitter cycles	JITER:DDP
MDVP local shimmer	MDVP:SHIMMER
MDVP local shimmer in dB	MDVP:SHIMMER(DB)
Three-point amplitude perturbation quotient	SHIMMER:APQ3
Five-point amplitude perturbation quotient	SHIMMER:APQS
MDVP 11-point amplitude perturbation quotient	MDVP:APQII
Average absolute differences between the amplitudes of consecutive periods,	SHIMMER:DDA
Noise-to-harmonics ratio	NHR
Harmonics-to-noise ratio	HNR

Table 1: Parameters Affecting the Movement of Muscles

The speech signals were recorded by the National Centre for Voice and Speech in Denver, Colorado, and Max Little of the University of Oxford worked together to create the dataset. A variety of biological voice measurements from 31 people, 23 of whom have Parkinson's disease, were part of this collection (PD). Amplitude metrics, Pulse metrics, Frequency metrics, Voicing metrics, Pitch metrics, and Harmonicity metrics are the six categories that Table 2 breaks down the parameters into. There are 195 instances in the collection. A specific voice measure is represented by each column in the table, and each row corresponds to one of the 195 voice recordings from these people. The "Status" parameter is the one that matters the most out of all the others because it is the only one that can tell healthy people from those who have Parkinson's disease apart. While a value of 0 indicates overall health, a value of 1 indicates Parkinson's disease. The sample data set that was used is depicted in table1.

id	age	MF0mean	MF0std	MF1mean	MF1std	MF2mean	MF2std	MF3mean	MF3std	MF4mean	MF4std	MF5mean	MF5std	MF6mean	MF6std	MF7mean	MF7std	MF8mean	MF8std	MF9mean	MF9std	MF10mean	MF10std	MF11mean	MF11std	MF12mean	MF12std	MF13mean	MF13std	MF14mean	MF14std	MF15mean	MF15std	MF16mean	MF16std	MF17mean	MF17std	MF18mean	MF18std	MF19mean	MF19std	MF20mean	MF20std	MF21mean	MF21std	MF22mean	MF22std	MF23mean	MF23std	MF24mean	MF24std	MF25mean	MF25std	MF26mean	MF26std	MF27mean	MF27std	MF28mean	MF28std	MF29mean	MF29std	MF30mean	MF30std	MF31mean	MF31std	MF32mean	MF32std	MF33mean	MF33std	MF34mean	MF34std	MF35mean	MF35std	MF36mean	MF36std	MF37mean	MF37std	MF38mean	MF38std	MF39mean	MF39std	MF40mean	MF40std	MF41mean	MF41std	MF42mean	MF42std	MF43mean	MF43std	MF44mean	MF44std	MF45mean	MF45std	MF46mean	MF46std	MF47mean	MF47std	MF48mean	MF48std	MF49mean	MF49std	MF50mean	MF50std	MF51mean	MF51std	MF52mean	MF52std	MF53mean	MF53std	MF54mean	MF54std	MF55mean	MF55std	MF56mean	MF56std	MF57mean	MF57std	MF58mean	MF58std	MF59mean	MF59std	MF60mean	MF60std	MF61mean	MF61std	MF62mean	MF62std	MF63mean	MF63std	MF64mean	MF64std	MF65mean	MF65std	MF66mean	MF66std	MF67mean	MF67std	MF68mean	MF68std	MF69mean	MF69std	MF70mean	MF70std	MF71mean	MF71std	MF72mean	MF72std	MF73mean	MF73std	MF74mean	MF74std	MF75mean	MF75std	MF76mean	MF76std	MF77mean	MF77std	MF78mean	MF78std	MF79mean	MF79std	MF80mean	MF80std	MF81mean	MF81std	MF82mean	MF82std	MF83mean	MF83std	MF84mean	MF84std	MF85mean	MF85std	MF86mean	MF86std	MF87mean	MF87std	MF88mean	MF88std	MF89mean	MF89std	MF90mean	MF90std	MF91mean	MF91std	MF92mean	MF92std	MF93mean	MF93std	MF94mean	MF94std	MF95mean	MF95std	MF96mean	MF96std	MF97mean	MF97std	MF98mean	MF98std	MF99mean	MF99std	MF100mean	MF100std	MF101mean	MF101std	MF102mean	MF102std	MF103mean	MF103std	MF104mean	MF104std	MF105mean	MF105std	MF106mean	MF106std	MF107mean	MF107std	MF108mean	MF108std	MF109mean	MF109std	MF110mean	MF110std	MF111mean	MF111std	MF112mean	MF112std	MF113mean	MF113std	MF114mean	MF114std	MF115mean	MF115std	MF116mean	MF116std	MF117mean	MF117std	MF118mean	MF118std	MF119mean	MF119std	MF120mean	MF120std	MF121mean	MF121std	MF122mean	MF122std	MF123mean	MF123std	MF124mean	MF124std	MF125mean	MF125std	MF126mean	MF126std	MF127mean	MF127std	MF128mean	MF128std	MF129mean	MF129std	MF130mean	MF130std	MF131mean	MF131std	MF132mean	MF132std	MF133mean	MF133std	MF134mean	MF134std	MF135mean	MF135std	MF136mean	MF136std	MF137mean	MF137std	MF138mean	MF138std	MF139mean	MF139std	MF140mean	MF140std	MF141mean	MF141std	MF142mean	MF142std	MF143mean	MF143std	MF144mean	MF144std	MF145mean	MF145std	MF146mean	MF146std	MF147mean	MF147std	MF148mean	MF148std	MF149mean	MF149std	MF150mean	MF150std	MF151mean	MF151std	MF152mean	MF152std	MF153mean	MF153std	MF154mean	MF154std	MF155mean	MF155std	MF156mean	MF156std	MF157mean	MF157std	MF158mean	MF158std	MF159mean	MF159std	MF160mean	MF160std	MF161mean	MF161std	MF162mean	MF162std	MF163mean	MF163std	MF164mean	MF164std	MF165mean	MF165std	MF166mean	MF166std	MF167mean	MF167std	MF168mean	MF168std	MF169mean	MF169std	MF170mean	MF170std	MF171mean	MF171std	MF172mean	MF172std	MF173mean	MF173std	MF174mean	MF174std	MF175mean	MF175std	MF176mean	MF176std	MF177mean	MF177std	MF178mean	MF178std	MF179mean	MF179std	MF180mean	MF180std	MF181mean	MF181std	MF182mean	MF182std	MF183mean	MF183std	MF184mean	MF184std	MF185mean	MF185std	MF186mean	MF186std	MF187mean	MF187std	MF188mean	MF188std	MF189mean	MF189std	MF190mean	MF190std	MF191mean	MF191std	MF192mean	MF192std	MF193mean	MF193std	MF194mean	MF194std	MF195mean	MF195std	status
0.0113	0.02971	0.06545	0.0...	21...	1	0.41	0.0...	4.813...	0.2664...	2...	0...																																																																																																																																																																																																																																																																																																																																																																																															
0.04518	0.04368	0.09403	0.0...	19...	1	0.45	0.0...	4.075...	0.33559	2...	0...																																																																																																																																																																																																																																																																																																																																																																																															
0.01058	0.0359	0.0827	0.0...	20...	1	0.42	0.0...	4.443...	0.3111...	2...	0...																																																																																																																																																																																																																																																																																																																																																																																															
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0.00940	0.01256	0.02487	0.0...	26...	1	0.63	0.7...	6.1676	0.1817...	2...	0...																																																																																																																																																																																																																																																																																																																																																																																															
0.01272	0.01717	0.03218	0.0...	23...	1	0.43	0.7...	5.498...	0.2277...	2...	0...																																																																																																																																																																																																																																																																																																																																																																																															
0.01725	0.02444	0.04324	0.0...	23...	1	0.54	0.7...	5.011...	0.1259...	2...	0...																																																																																																																																																																																																																																																																																																																																																																																															

Figure 2: Vocal Features of the Dataset

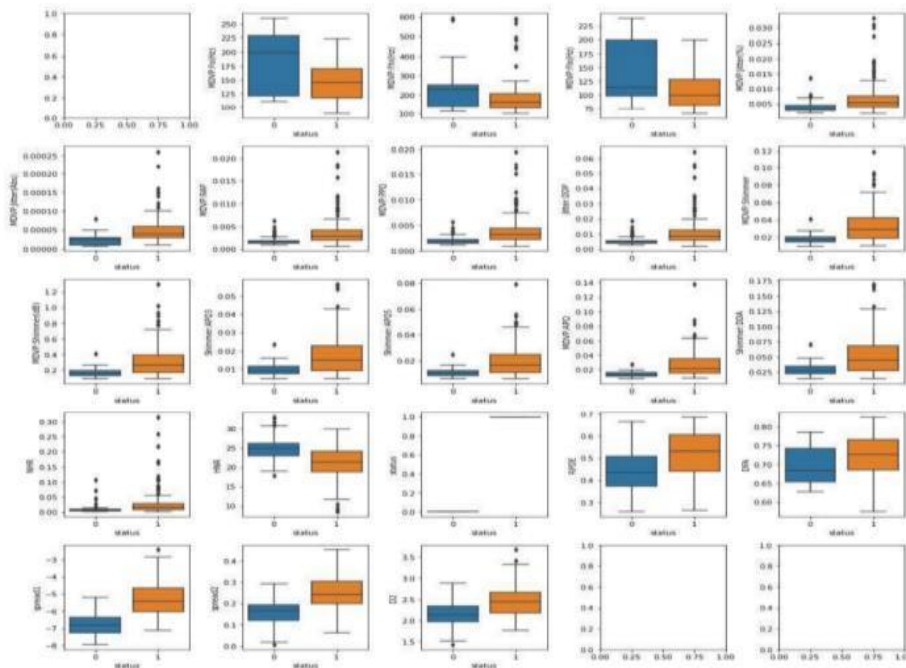


Figure 3: Graphical Representation of Disease Characteristics V/S the Status of the Person

III. BLOCK DIAGRAM

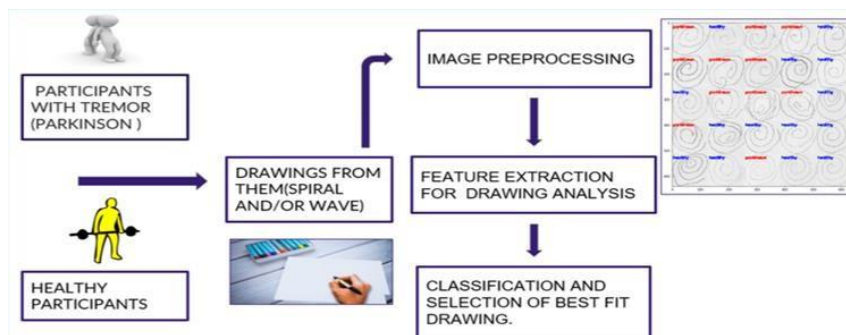


Figure 4: Flow Chart for Classification and Testing

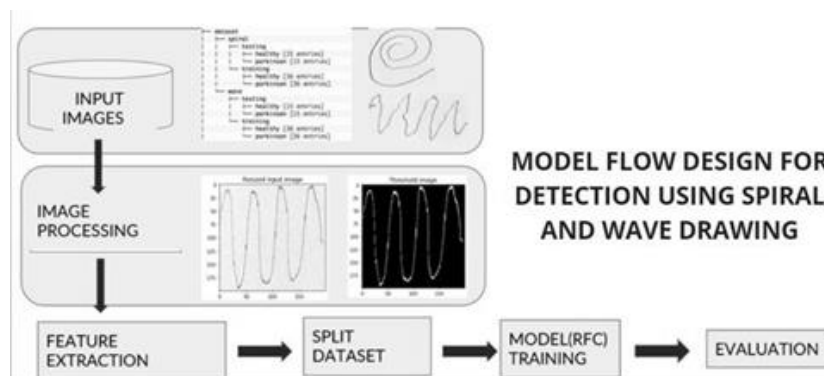


Figure 5: Flow Design for Detection using Spiral and Wave Drawing

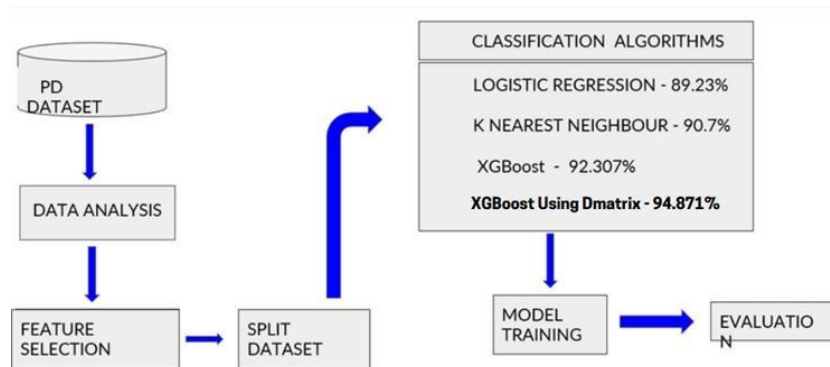


Figure 6: Design Flow for Voice Detection of affected person

IV. RESULTS AND DISCUSSIONS

The Parkinson Dataset (PD dataset) parameters are classified into 5 categories namely i) Frequency parameters, ii) Pitch parameters, iii) Amplitude Parameters, iv) Voicing Parameters, v) Pulse parameters. The parameter values are then analyzed to identify outliers and errand values, padded with zero for empty values and removal of the parameter which are not contributing for classification. The data set was split into test and training data to train the model, it was trained on different classification algorithms which has functions that balances the characteristics of the input so that the output separates one class with positive traits and the other into negative. The dataset was subjected to the following different classification algorithms:

- 1. Logistic regression:** As logistic regression only uses log function which statistically is a logit transformation applied to the data. The performance is calculated as the ratio of probability of success to the probability of failure. Logistic regression does not show very trust worthy results. The accuracy was 89.23%.
- 2. K-Nearest Neighbor (KNN):** K-Nearest Neighbour algorithm expects large amount of training data to give benefiting result, as The K-NN algorithm puts the new entity in the category that is most similar to the existing classes on the premise that the new case/data and the current cases are comparable. Due to availability of small dataset of this disease, the algorithm was capable of producing an accuracy of. 90.7%.

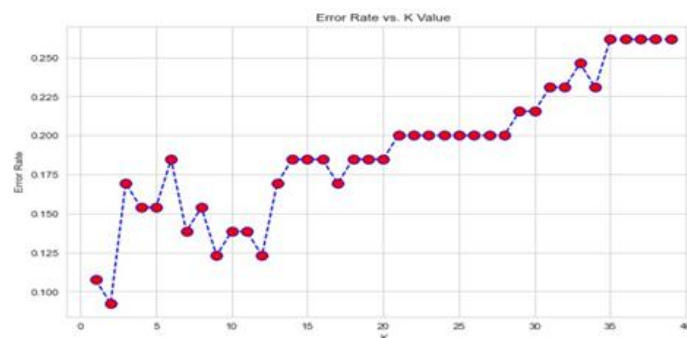


Figure 7: Results using KNN Algorithm

3. **Random forest:** Collectively, Random Decision Forest is a classification learning process and uses regression and other tasks during training to build a large number of decision trees. When Random Forest regression model was employed for the PD dataset, it provided an accuracy of 86.15%, which was quite less when compared to other algorithms.
4. **XGBoost:** The next promising classification algorithm was XGBoost is a distributed gradient boosting library developed to be very portable, effective, and flexible. It uses Gradient Boosting framework and implements classification learning algorithms. The distributed gradient boosting library is efficient for small datasets and it gave us an approximate accuracy of 92.30%.

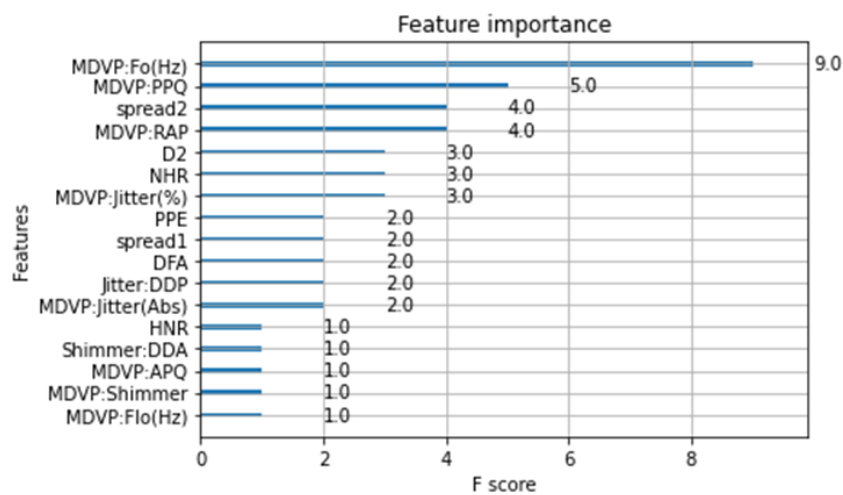


Figure 8: Results using XGBoost Algorithm

5. **XGBoost Using Dmatrix:** XGBoost when it employed DMatrix showed the most efficient and accurate results. XGBoost utilises an internal data structure that is designed for both memory effectiveness and training speed in DMatrix. XGBoost with DMatrix provided a high accuracy of 94.871% and a precision of 88.88%. We must use the DMatrix format as the model and convert our PD dataset into the format so that XGBoost can use in order for it to work.

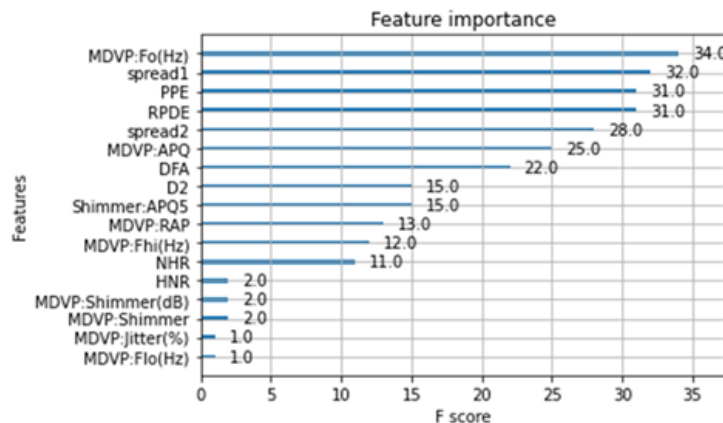


Figure 9: Results using XGBoost with D-Matrix Algorithm

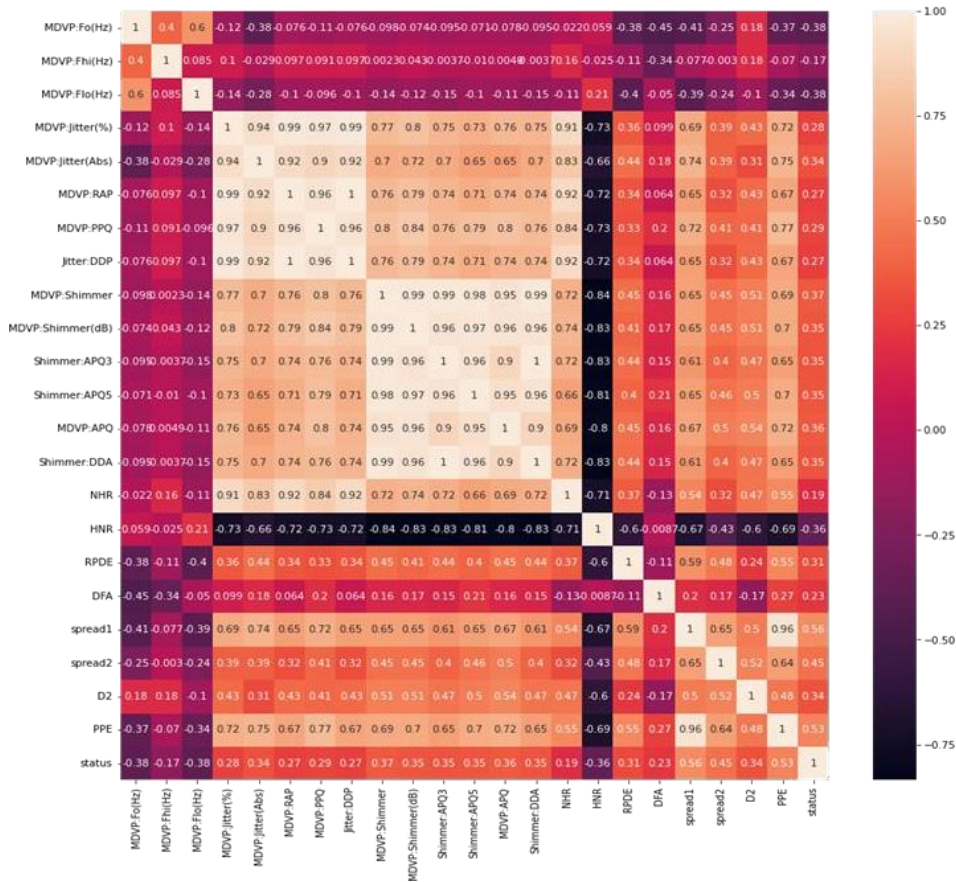


Figure 10: Heatmaps using XGBoost with D-Matrix Algorithm

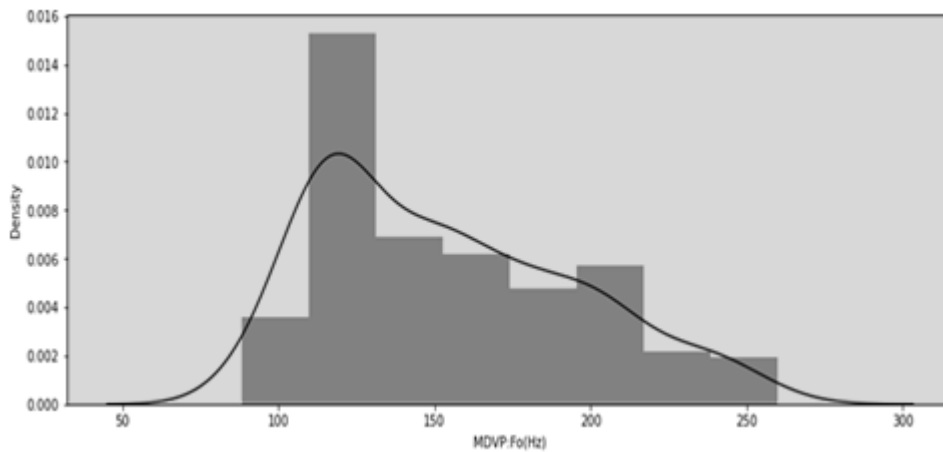


Figure 11: Graphs using XGBoost with D-Matrix Algorithm

V. CONCLUSION

For the patient to obtain the right care and decrease the consequences of Parkinson's disease, the condition must be recognised as soon as feasible. In this study, we propose an artificial intelligence-powered prediction model that is used to increase the

precision of disease diagnosis in people and enable early detection. We intend to aid physicians in accurately diagnosing and forecasting Parkinsons Disease, The two activities that are currently challenging for them to do due to the present method of diagnosis process is the ability to accurately detect and further provide prediction. We divided the task of detection and prediction, and we used that data in a neural model to pinpoint and quantify the region of the brain that is impacted.

The proposed technique resulted in accuracy of 94.871%, sensitivity of 100%, and specificity of 88%. The research has made the following contributions: (i) This model is quite helpful to doctors as it only makes use of five features. (ii) Because of the substantial and consistent sample that was applied, this model is precise. (iii) By using neural networks and image processing separately, this process uses relatively minimal system resources and has reliable accuracy, which makes it simpler to apply this model to real-world applications. According to the proposed model, objective evaluation and the use of fundamental neural networks are useful in the development of prediction models that can help a doctor diagnose a patient more efficiently and with a smaller chance of human error.

VI. FUTURE SCOPE

Compared to earlier approaches, the model presented in this study took a distinct approach to the problem of Parkinson's disease recognition, but the outcomes are still highly applicable to real-world conditions. Although the conclusions are factual, The model must be improved and used in circumstances that actually occur in the real world. These results are not the end aim. A model with more records in the dataset can deliver better accuracy and more reliable. The effectiveness of this approach can also be more clearly demonstrated by evaluating it with established approaches in term of accuracy, effectiveness and applicability in real-world circumstances. With the use of this technique, clinicians will be able to identify Parkinson's disease more precisely than before. More research may be done on datasets to include more relevant information and include more variables that reflect the disease. Lack of awareness is a major contributing factor to this illness, as is the fact that complications often appear or become apparent only after the person has already begun to experience neuronal degeneration for a while. Hence, datasets generated from patients taken earlier than one week if documented, can generate better outcomes.

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